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Technical Alarms During Continuous ECG Monitoring in the Intensive Care Unit

An analysis of technical alarms to guide hospital-based alarm management strategies and inform monitoring manufacturers on needed improvements to technical alarm algorithms used in bedside ECG monitors.



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Introduction

Hospital-based electrocardiographic (ECG) monitors are configured to alarm for a number of different types of arrhythmias, ST-segment changes, and QT interval lengths that are designed to alert busy nurses. However, accurate detection of ECG abnormalities/features requires a clean signal. Most ECG devices include technical and/or inoperative alarm algorithms that are designed to notify and inform the nurse when a specific signal quality issue arises to minimise monitoring interruptions. For example, one type of technical alarm is ECG lead off (single or multiple), or ECG leads fail (no signal) that informs the nurse to replace either the skin-electrode(s) and/or the lead wire(s). Technical alarms can be configured to either generate an alarm sound (e.g., warning, continuous foghorn tone) or as an inaudible text message alert that flashes on the bedside monitoring screen. While there are no established guidelines for optimal alarm settings, technical alarms for artefact (noisy signal) or when a single ECG lead is off are typically configured as inaudible text message alerts (flash text on the bedside monitor); thus, they do not need to be silenced by the nurse. In general, inaudible text is selected for these types of alarms because there is still an ECG signal present; thus, arrhythmia detection is maintained. Many hospitals choose to configure some more important technical alarm types using an audible alarm configuration to ensure that a clean ECG signal is established promptly. For instance, when more than one ECG lead is off, or there is an extended period of time in a technical alarm condition

(sustained artefact), an audible alarm is used since both of these types of technical issues may turn off or suspend arrhythmia detection software and an arrhythmia could be missed.

While technical alarms (i.e., artefact, ECG lead(s) fail, ECG lead(s) off) are designed to ensure optimal ECG signal quality for arrhythmia detection, these types of alarms are extremely common and can contribute to alarm fatigue in nurses. In a comprehensive one-month ECG alarm study in 461 intensive care unit (ICU) patients of the more than 2.5 million total alarms generated, 32% (791,632) were technical alarms (Drew et al. 2014). Alarm fatigue associated with bedside ECG and physiologic (vitals sign) monitors can create the following unsafe situations in patient care: (1) inadvertently ignoring alarms due to desensitisation (i.e., alarm noise is assimilated into a nurses' workflow); (2) lowering the volume of alarms to reduce patient and family stress from alarm noise; (3) completely silencing alarms; and/or (4) delayed response to alarms (Bonafide and et al. 2015). Additionally, nurses often experience overload in various forms during their work (e.g., cognitive and physical), which is further compounded by ECG device-related alarm fatigue (Lewandowska et al. 2020).

Alarm fatigue and the related responses set the stage for a major patient safety issue, which has devastating effects on both nurses and patients. Alarm fatigue has been associated with over 650 hospital deaths (Dee et al. 2022; Ruskin and Hueske-Kraus 2015), and in a retrospective study from 2011, there were 216 patient deaths



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linked to issues with alarm fatigue (Shue and Ortiz 2019). Importantly, these data are dated, and because few substantive interventions have been introduced to solve alarm fatigue, morbidity and mortality are likely much higher.

There have been several hospital-based studies that have evaluated technical alarms generated from ECG monitors (Albert et al. 2015; Cvach et al. 2013; Drew et al. 2014; Graham and Cvach 2010; Sendelbach et al. 2015; Shue and Ortiz 2019; Watanakeeeree et al. 2021). One observational study conducted in adult ICU patients showed that 32% (791,632) of more than 2.5 million total alarms were technical alarms, and the vast majority (358,277) were for artefact followed by single ECG lead fail (90,547) (Drew et al. 2014). Technical alarms for arrhythmia suspend and ECG leads off (no signal) were not reported. In a subsequent secondary data analysis from this study, artefact, ECG leads off/fail, and arrhythmia suspend were reported in ICU patients with a left ventricular assist device (Watanakeeeree et al. 2021). Artefact was the most common technical alarm (96%) followed by ECG leads fail (3.5%) and then arrhythmia suspend (0.5%). Of the remaining studies, technical alarms were examined at pre- and post-quality improvement (QI) project implementation

(Cvach et al. 2013; Graham and Cvach 2010; Sendelbach et al. 2015; Shue and Ortiz 2019), and one examined alarm rates when using disposable versus non-disposable ECG lead wires (Albert et al. 2015). Two studies examined both artefact and ECG leads off/fail alarms (Albert et al. 2015; Sendelbach et al. 2015), two examined both ECG leads off and arrhythmia suspend (Cvach et al. 2013; Graham and Cvach 2010), and one examined only ECG leads off (Shue and Ortiz 2019). To our knowledge, no study has examined specific technical alarm types in a comprehensive manner (i.e., types, duration, possible patient/clinical factors). A more extensive analysis of technical alarms for these characteristics may help guide hospital-based alarm management strategies and inform monitoring manufacturers on needed improvements to technical alarm algorithms used in bedside ECG monitors.

Purpose

The purpose of this study was twofold: (1) examine the number, type, and duration of technical alarms for artefact; arrhythmia suspend, and ECG leads fail, and (2) examine whether demographic (age, sex, race) factors, clinical features (body mass index, impaired cognitive status, tremor, smoking), mechanical ventilation and/or ICU type (cardiac, medical/surgical, or neurological,) are associated with technical alarms.

Methods

Study Design

This was a secondary data analysis using data from a comprehensive one-month alarm study among a consecutive cohort of adult intensive care unit patients (Drew et al. 2014). The occurrence rate, type, and clinical features hypothesised to increase the occurrence of technical alarms (described below) for the artefact, arrhythmia suspend, and ECG leads fail were examined for this analysis. The Institutional Review Board (IRB) approved the study (IRB# 12-09723) with a waiver of patient consent because the alarm data was captured in

the background, did not interrupt patient care, and was analysed retrospectively.

Sample and Setting

The primary study included 461 consecutive adult ICU patients with continuous ECG monitoring from three types of ICUs, including cardiac (16 beds), medical/surgical (32 beds), and neurological (29 beds), at a large tertiary-quaternary medical centre over a 31-day period. For this study, based on our prior work (Bawua et al. 2022; Drew et al. 2014; Harris et al. 2017; Suba et al. 2019), we hypothesised that BMI, being a current smoker, having cognitive impairment, a tremor, or mechanical ventilation would be associated with a higher rate of technical alarms. There were five patients (1.08%) who did not have BMI documented and were subsequently excluded, leaving 456 ICU patients available for analysis. Demographics, including sex, age, race, and ethnicity, were obtained from the electronic health record (EHR). Additionally, ICU type (cardiac, medical/surgical and neurological) and the use of mechanical ventilation were acquired from the EHR.

Alarm Data Capture System

Our data capture system has been described in detail previously (Drew et al. 2014; Pelter et al. 2023). Briefly, all ECG and physiologic monitor waveforms (i.e., seven ECG channels [I, II, III, aVR, aVL, and aVF], arterial blood pressure, pulse oximetry [SpO₂], impedance respirations), numeric vital signs, and alarm types (both audible and inaudible) were acquired via a secure data capture system. Data were downloaded to a secure research server approved by our hospital and were extracted into Extensible Markup Language (XML) files for analysis.

Technical Alarm Types

Technical alarm types, called system status alarms by the vendor, we examined included: (1) artefact (noisy signal); (2) arrhythmia suspend (no arrhythmia detection [software off] due to sustained artefact >20 seconds in the prior 30 seconds); and (3) ECG leads fail (no discernible ECG waveform displayed). **Figure 1** shows the

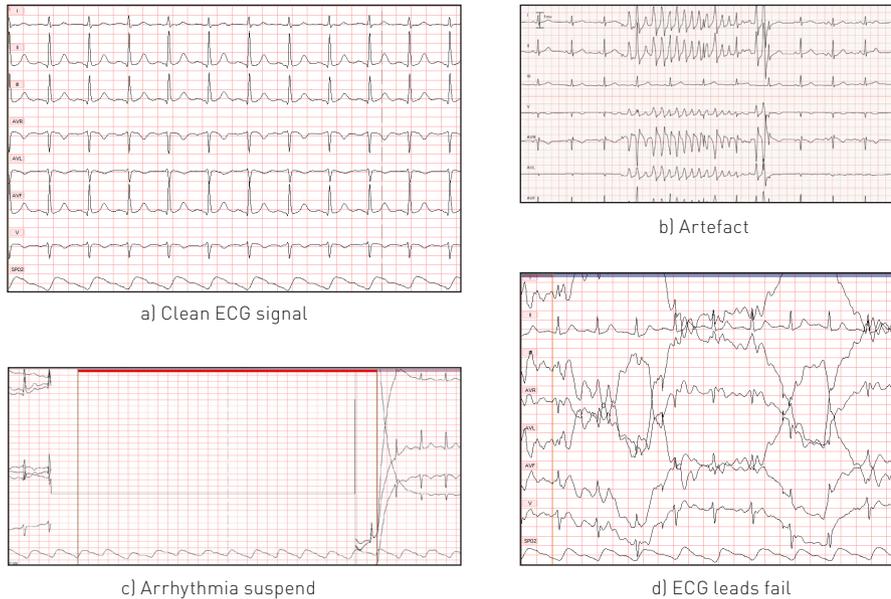


Figure 1. Three types of technical alarms: a) clean ECG signal; b) artefact; c) arrhythmia suspend; and d) ECG leads fail. Shown on each ECG (top to bottom) are leads I, II, III, V (V1), aVR, aVL, aVF and SpO₂ except B).

type of technical alarms examined, as well as a clean signal ECG. Technical alarms greater than 20 minutes in duration were excluded as we assumed that this likely indicated that the patient was not being monitored (e.g., procedure on/off unit, bathing, etc.), but the monitor had not been paused. Alarms for artefact were configured in the bedside monitor as an inaudible text message alert. In this alarm condition, full arrhythmia processing is suspended while the lethal arrhythmia algorithm is still active. However, its accuracy may be hindered by the artefact. Alarms for arrhythmia suspend and ECG leads (plural) fail were configured as an audible warning alarm. In these alarm conditions, a repeating foghorn tone sounds, and arrhythmia analysis is suspended until the technical alarm condition is resolved.

Data Analysis

Descriptive statistics were used to describe sample demographics, factors hypothesised to increase the rate of technical alarms, ICU type, length of ICU stay (hours), and frequency and duration of each technical alarm. Descriptive statistics are reported as frequencies for categorical variables

and mean $\hat{\mu} \pm$ standard deviation (SD) for continuous variables. Data were tabulated in the overall sample and grouped based on the type of technical alarm. For the statistical analysis, we used medians and interquartile ranges (IQRs) due to the high variability in the number of technical alarms a patient may have generated. For this analysis, IQRs were weighted (weighted median, weighted 25th percentile, weighted 75th percentile) by ICU monitoring time. A negative binomial GLM regression model was used to evaluate both univariate and multivariate associations because of the variability of alarm counts per patient. A p-value of <0.05 was used as the critical value to determine statistical significance. All statistical analyses were conducted using R (v4.3.2; R Core Team 2023).

As mentioned above, due to high variability in the number of all technical alarm types (i.e., one patient could have one while another patient could have hundreds), we used the following approach: (1) occurrence rates for each alarm type were calculated per 10 hours of monitoring; (2) median and 25th and 75th percentiles of the distribution were weighted by monitoring time, and; (3) a chi-square test was used to test

for deviance of the binomial GLM, where a p-value of <0.05 was used to determine statistical significance. Predictors in the multivariate model were included based on subject-matter knowledge and the conceptual model. For this study, based on our prior work (Drew and Harris et al., 2014; Bawua and Miaskowski et al., 2022; Suba and Sandoval et al., 2019), we hypothesised that BMI, being a current smoker, having cognitive impairment, a tremor, or mechanical ventilation would be associated with a higher rate of technical alarms; hence, only patients with these variables documented were examined.

Results

Entire Sample

Table 1 shows the 456 adult ICU patients included in the study. The total number of technical alarms was 572,763. Of the total, 557,018 (97%) were artefact alarms, 3,378 (0.6%) were arrhythmia suspend alarms, and 12,367 (2.2%) were ECG leads fail.

Patient Characteristics by Alarm Type

Each technical alarm type was compared by patient demographics, ICU type, clinical features, and mechanical ventilation as illustrated in **Table 2**. All but 5 ($n=451$, 99%) patients generated one or more artefact alarms, 233 (51%) arrhythmia suspend alarms and 438 (96%) ECG leads fail alarms. It's important to note that a single patient could have more than one type of technical alarm. Patients in either the medical surgical or neurological ICUs had the highest proportion of alarms as compared to the cardiac ICU, which again likely reflects the number of beds in each unit.

The proportion of the three technical alarm types compared by, age, sex, ethnicity, race, ICU type, BMI, current smoker, cognitive impairment, tremor, and mechanical ventilation were equivalent (**Table 2**). Due to high variability in the number of technical alarms, the median values are discussed here and were used in the statistical analysis described below. Median ICU monitoring hours was longest in the patients with arrhythmia suspend

Variable of Interest	n (%)
Demographics n=456	
Overall Age (mean ± SD, in years)	60 ± 17
Categories	
18 to 34	42 (9)
35 to 49	86 (19)
50 to 64	138 (30)
65 to 79	132 (29)
80 or older	58 (13)
Gender	
Female	208 (46)
Male	248 (54)
Ethnicity	
Hispanic	52 (11)
Non-Hispanic	396 (87)
Unable to state	8 (2)
Race	
Asian	74 (16)
Black or African American	35 (8)
Native Hawaiian or Pacific Islander	8 (2)
White	278 (61)
Unknown declined to state	61 (13)
Intensive Care Unit Type	
Cardiac (16 beds)	81 (18)
Medical Surgical (32 beds)	180 (40)
Neurological (29 beds)	195 (43)
Factors Hypothesised to Increase the Rate of Technical Alarms	
Body Mass Index (kg/m ²)	28.1 + 8
Cognitive Impairment	195 (43)
Current Smoker	69 (15)
Mechanical Ventilation	179 (39)
Tremor	35 (8)
Intensive Care Unit Length of Stay (hours)	
Mean + SD	98.54 + 121
Median (IQR)	51 (26 – 113)
Number and Type of Technical Alarm	
Total of All Types	572,763
Artefact	557,018 (97.3)
Arrhythmia Suspend	3,378 (0.59)
ECG Leads Fail	12,367 (2.2)

Table 1. Demographics and clinical features of the 456 adult intensive care unit patients with technical alarms during continuous ECG monitoring.

Variable of Interest N=456 ICU Patients	Artefact 557,018 Alarms 451 Patients n (%)	Arrhythmia Suspend 3,378 Alarms 233 Patients n (%)	ECG Leads Fail 12,367 Alarms 438 Patients n (%)
Age (mean ± SD, in years)	60 ± 17	60 ± 18	59 ± 17
Sex (self-identified)			
Female	205 (46)	101 (43)	196 (45)
Male	246 (55)	132 (57)	242 (55)
Ethnicity			
Hispanic	52 (12)	27 (11)	51 (12)
Non-Hispanic	91 (86)	202 (86)	379 (86)
Unable to state	8 (2)	4 (2)	8 (2)
Race			
Asian	73 (16)	40 (17)	71 (16)
Black or African American	34 (8)	21 (9)	35 (8)
Native Hawaiian or Pacific Islander	8 (2)	5 (2)	8 (2)
White	275 (61)	138 (59)	264 (60)
Unable to state	61 (13)	29 (12)	60 (14)
ICU Type			
Cardiac (16 beds)	81 (18)	38 (16)	79 (18)
Medical Surgical (32 beds)	178 (39)	98 (42)	175 (40)
Neurological (29 beds)	192 (43)	97 (42)	184 (42)
Variables Hypothesised to Increase rate of Technical Alarms			
Body Mass Index (kg/m ²)	28 + 8	28 + 8	28 + 8
Current Smoker	68 (15)	36 (16)	65 (15)
Cognitive Impairment	193 (43)	118 (51)	189 (43)
Tremor	35 (8)	27 (12)	35 (8)
Mechanical Ventilation	178 (40)	104 (45)	177 (40)
Monitoring Hours in ICU			
Mean + SD	99 + 121	144 + 149	102 + 123
Median	51	91	53
Minimum and Maximum	3 – 743	3 – 743	5 – 743
Number of Alarms			
Mean	1235 + 2568	15 + 31	28 + 59
Median (IQR)	363 (138 – 1,160)	4 (2 – 4)	9 (4 – 28)
Minimum - Maximum	1 – 21,752	1 – 256	0 – 795
Time in Alarm Condition During ICU Monitoring (minutes:seconds)			
Mean + SD	67:35 + 69	10:09 + 26	19:42 + 34
Median (IQR)	19:20 (6:42 – 60:39)	2:06 (0:34 – 9:03)	9:26 (3:09 – 22:56)

Table 2. Frequency of technical alarms in 456 ICU patients by type: artefact, arrhythmia suspend, and ECG leads fail compared by demographics, clinical features, ICU unit type and mechanical ventilation. Note: a patient could have more than one type of technical alarm.

alarms (91 hours), followed by ECG leads fail (53 hours), then artefact (51 hours). The highest median number of alarms was for artefact (363), followed by ECG lead fail (9), then arrhythmia suspend (4).

The median time in an alarm condition was highest for artefact (19:20 min:sec), followed by ECG leads fail (9:26 min:sec), then arrhythmia suspend (2:06 min:sec).

Duration of Technical Alarms

Most of the technical alarms were two seconds in length, specifically, 58% (n=323,070) of the artefact alarms, 60.5%

Technical Alarm Type	Duration Category		
	2 sec to <5 min	5 min to <10 min	10 min to <15 min
Artefact 557,018 Alarms	552,561 [99.2]	3,343 [0.6]	1,114 [0.2]
Arrhythmia Suspend 3,378 Alarms	3,358 [99.4]	17 [0.5]	3 [0.1]
ECG Leads Fail 12,367 Alarms	12,293 [99.4]	50 [0.4]	24 [0.2]

Table 3. Technical alarms in 456 intensive care unit patients grouped by duration categories

Artefact Alarm Rates ¹				
Characteristics	n=456	Median ²	(IQR) ²	p-value ³
Age, y.				0.08
18 to 34	42	94.7	[20.6 - 194.0]	
35 to 49	86	108.3	[39.6 - 169.9]	
50 to 64	138	99.8	[56.4 - 185.5]	
65 to 79	132	67.4	[23.2 - 135.2]	
80 plus	58	106.0	[28.2 - 148.3]	
Gender				0.60
Female	208	93.0	[40.0 - 165.0]	
Male	248	84.7	[36.9 - 175.7]	
Race				0.50
Asian	74	89.4	[26.2 - 164.9]	
Black or African American	35	67.2	[48.9 - 115.9]	
Native Hawaiian or Pacific Islander	8	77.8	[50.5 - 111.9]	
White	278	95.9	[35.0 - 196.7]	
Unknown or decline to state	61	86.2	[49.0 - 121.1]	
ICU Type				0.25
Neurological	195	86.2	[38.9 - 144.0]	
Medical-Surgical	180	99.3	[38.8 - 185.6]	
Cardiac	81	79.6	[23.3 - 173.1]	
BMI (kg/m²)				0.13
<25	183	88.7	[31.6 - 199.1]	
25-30	131	98.7	[37.4 - 160.9]	
30+	142	73.8	[42.7 - 134.6]	
Smoker				<0.001
No	387	77.8	[32.4 - 165.0]	
Yes	69	121.1	[78.0 - 180.7]	
Cognitive Impairment				0.41
No documented cognitive problem	261	83.9	[35.7 - 159.5]	
Cognitive problem documented	195	86.2	[37.1 - 185.6]	
Tremor				<0.001
No or undocumented	421	80.6	[35.4 - 150.9]	
Yes	35	197.5	[73.8 - 390.0]	
Mechanical Ventilation				0.01
No	277	112.8	[50.4 - 207.5]	
Yes	179	76.7	[30.9 - 137.1]	

Table 4. Occurrence rates of technical alarms for artefact by demographic, ICU type and factors hypothesised to increase the number of technical alarms in 456 ICU patients. ¹Rate is per 10 hours of monitoring. ²Median and 25th and 75th percentiles of the distribution are weighted by monitoring time. ³Chi-squared test for deviance of negative binomial GLM with single characteristic as predictor versus null model.

(n=2,044) of arrhythmia suspend alarms and 64% (n=7,915). Each type of technical alarm was categorised into duration time frames using the following categories, which could help guide alarm configuration delays and/or algorithm development: two seconds to <five minutes, five minutes to <10 minutes, and 10 minutes to <15 minutes. As shown in Table 3, 99% of all of the technical alarm types were in the two seconds to <five-minute category.

Univariate and Multivariate Analysis

Below we describe the univariate and multivariate analysis for each technical alarm type.

Artefact: In the univariate analysis, being a current smoker and having a tremor was associated with higher rates of artefact alarms. Being treated with mechanical ventilation was associated with fewer alarms (Table 4). Figure 2 shows a forest plot of the multivariate analysis. Being a current smoker and having a tremor remained significant predictors of artefact alarms. Patients treated with mechanical ventilation were less likely to have artefact alarms. All of the other variables included were not significant.

Arrhythmia Suspend: In the univariate analysis, being a current smoker, having cognitive impairment and having a tremor was associated with higher rates of arrhythmia suspend alarms. Being treated with mechanical ventilation was associated with fewer alarms (Table 5). Figure 2 shows a forest plot of the multivariate analysis. Being a current smoker, having cognitive impairment and having a tremor remained significant predictors of arrhythmia suspend alarms. Being treated with mechanical ventilation was associated with fewer alarms. All of the other variables included were not significant.

ECG Leads Fail: In the univariate analysis, age, race and having a tremor were associated with higher rates of ECG leads fail alarms. Being a current smoker, having cognitive impairment, and treatment with mechanical ventilation were not significant (Table 6). Figure 2 shows a forest plot of the multivariate analysis. The race category

Arrhythmia Suspend Alarm Rates ¹				
Characteristics	n=456	Median ²	(IQR) ²	p-value ³
Age, y.				0.10
18 to 34	42	0.3	[0.0 - 0.9]	
35 to 49	86	0.3	[0.0 - 0.8]	
50 to 64	138	0.4	[0.1 - 0.9]	
65 to 79	132	0.2	[0.0 - 0.4]	
80 plus	58	0.2	[0.0 - 0.4]	
Gender				0.07
Female	208	0.3	[0.0 - 0.6]	
Male	248	0.2	[0.0 - 0.8]	
Race				0.07
Asian	74	0.2	[0.0 - 0.4]	
Black or African American	35	0.2	[0.0 - 0.5]	
Native Hawaiian or Pacific Islander	8	0.1	[0.1 - 0.2]	
White	278	0.3	[0.0 - 0.9]	
Unknown or decline to state	61	0.3	[0.0 - 0.6]	
ICU Type				0.49
Neurological	195	0.2	[0.0 - 0.4]	
Medical-Surgical	180	0.3	[0.0 - 0.8]	
Cardiac	81	0.3	[0.0 - 1.0]	
BMI (kg/m2)				0.17
<25	183	0.2	[0.0 - 0.9]	
25-30	131	0.2	[0.0 - 0.8]	
30+	142	0.3	[0.0 - 0.6]	
Smoker				<0.001
No	387	0.2	[0.0 - 0.6]	
Yes	69	0.5	[0.1 - 0.9]	
Cognitive Impairment				0.007
No documented cognitive problem	261	0.1	[0.0 - 0.7]	
Cognitive problem documented	195	0.3	[0.1 - 0.8]	
Tremor				<0.001
No or undocumented	421	0.2	[0.0 - 0.6]	
Yes	35	1.0	[0.3 - 2.7]	
Mechanical Ventilation				0.009
No	277	0.3	[0.0 - 0.9]	
Yes	179	0.2	[0.0 - 0.6]	

Table 5. Occurrence rates of arrhythmia suspend alarms by demographic, ICU type and factors hypothesised to increase the number of technical alarms in 456 ICU patients. ¹Rate is per 10 hours of monitoring. ²Median and 25th and 75th percentiles of the distribution are weighted by monitoring time. ³Chi-squared test for deviance of negative binomial GLM with single characteristic as predictor versus null model.

of Native Hawaiian/Pacific Islander and unknown race (patient unable to state due to acute illness) were significant predictors of ECG lead fails alarms, but the sample was small. In addition, being treated in the cardiac ICU, having cognitive impairment,

and having a tremor remained significant predictors of ECG leads fail alarms. Being treated with mechanical ventilation was associated with fewer alarms. All of the other variables included were not significant.

Discussion

To our knowledge, this is the first study to examine factors associated with three types of technical alarms, specifically artefact, arrhythmia suspend, and ECG leads fail, in 456 consecutive ICU patients. Artefact represented the vast majority of alarms, 97%, followed by ECG leads fail, 2.2%, then arrhythmia suspend, 0.5%. Fifty-eight percent of artefact alarms and more than 60% of arrhythmia suspend, and ECG leads fail alarms were two seconds in duration. Patients who were current smokers at admission were more likely to have artefact (1.16 times more likely) and arrhythmia suspend (1.98 times more likely) alarms. Having a tremor was associated with all three types of technical alarms (1.91 times more likely for artefact; 3.78 times more likely for arrhythmia suspend; and 1.84 times more likely for ECG leads fail). Documented cognitive impairment was associated with arrhythmia suspend (1.63 times more likely) and ECG leads fail alarms (1.30 times more likely). Being treated with mechanical ventilation was associated with fewer alarms for all three types of technical alarms.

Artefact

Of seven prior published studies that we identified as relevant to compare with our study, artefact was reported in four (Albert et al. 2015; Drew et al. 2014; Watanakeeree et al. 2021). Two were associated with this secondary data analysis and report the same findings as our study (e.g., the artefact was the most common type). Of the two remaining studies, one did not report specifically on artefact alarms but rather grouped artefacts with other types of alarms (Sendelbach et al. 2015). However, Albert et al. (2015) did report on artefact alarms. In their study, artefact alarm rates were examined by ECG lead wire type (disposable versus reusable) in 1,611 unique cardiac telemetry unit patients with 2,330 admissions. They found that artefact alarms were the second most common type of technical alarm (ECG leads off/fail most common), which is different than our study, where we found the artefact was by far the most common alarm. Their study

ECG Leads Fail Alarm Rates ¹				
Characteristics	n=456	Median ²	(IQR) ²	p-value ³
Age, y.				0.005
18 to 34	42	1.4	(1.0 - 2.9)	
35 to 49	86	1.8	(1.2 - 3.5)	
50 to 64	138	2.2	(1.3 - 3.2)	
65 to 79	132	1.6	(0.9 - 2.2)	
80 plus	58	1.7	(1.2 - 2.6)	
Gender				0.94
Female	208	1.7	(1.1 - 2.7)	
Male	248	1.7	(1.2 - 3.0)	
Race				<0.001
Asian	74	1.7	(1.0 - 2.1)	
Black or African American	35	1.2	(0.9 - 2.8)	
Native Hawaiian or Pacific Islander	8	1.6	(0.9 - 1.8)	
White	278	2.0	(1.3 - 3.4)	
Unknown or decline to state	61	1.6	(1.2 - 2.9)	
ICU Type				0.53
Neurological	195	1.7	(1.2 - 3.0)	
Medical-Surgical	180	1.7	(1.0 - 3.1)	
Cardiac	81	1.8	(1.3 - 2.7)	
BMI (kg/m2)				0.51
<25	183	1.6	(1.1 - 2.5)	
25-30	131	2.0	(1.1 - 3.3)	
30+	142	1.8	(1.2 - 3.3)	
Smoker				0.48
No	387	1.7	(1.1 - 2.8)	
Yes	69	2.2	(1.4 - 3.4)	
Cognitive Impairment				0.05
No documented cognitive problem	261	1.8	(1.2 - 2.7)	
Cognitive problem documented	195	1.7	(1.2 - 3.1)	
Tremor				<0.001
No or undocumented	421	1.7	(1.2 - 2.6)	
Yes	35	2.9	(1.5 - 5.6)	
Mechanical Ventilation				0.16
No	277	2.0	(1.2 - 3.1)	
Yes	179	1.7	(1.2 - 2.7)	

Table 6. Occurrence rates of electrocardiographic leads off by demographic, ICU type and factors hypothesized to increase the number of technical alarms in 456 ICU patients. ¹Rate is per 10 hours of monitoring. ²Median and 25th and 75th percentiles of the distribution are weighted by monitoring time. ³Chi-squared test for deviance of negative binomial GLM with single characteristic as predictor versus null model.

included cardiac telemetry unit patients, whereas ours included ICU patients. This may suggest that cardiac telemetry unit patients are more susceptible to leads off/fail, which is not entirely surprising given

that these patients are more mobile than ICU patients who are mostly in bed. It is worth noting that in their study, the rate of artefact versus ECG leads off/fail was similar (2,993 artefact versus 3,555),

suggesting that both types are common. Their study is interesting in that it showed that there were fewer artefact alarms in patients who had disposable ECG lead wires that were designed with a patented push-button feature. This study sheds light on one possible solution to reducing artefact alarms.

None of the studies examined patient-level factors associated with artefact alarms; hence, our study offers new information. We found that patients who were current smokers at admission or had tremors were more likely to have artefact alarms. Our study shows that patients with these characteristics may need more focused alarm management strategies and/or treatment(s). For example, the effects of nicotine withdrawal may need to be treated. Determining whether a tremor is part of the patient’s history could be useful, or if new, it may suggest untoward effects of medications (i.e., drug induced Parkinson’s) (Jeong et al. 2021; Shin and Chung 2012) Interestingly, being treated with mechanical ventilation was protective against artefact alarms. This is in contrast to prior studies our group has published showing that mechanical ventilation was associated with false arrhythmia and respiratory rate type alarms (Bawua et al. 2022; Harris et al. 2017). Sedation during mechanical ventilation may be one explanation, but this finding needs further investigation.

Arrhythmia Suspend

Of seven prior published studies that we identified as relevant to compare with our study, arrhythmia suspend was reported in three (Cvach et al. 2013; Graham and Cvach 2010; Watanakeeree et al. 2021). One was a secondary data analysis using our dataset that included only three patients with a left ventricular assist device. Arrhythmia suspend was the least common type, as was found in our study.

In a study by Cvach et al. (2013) arrhythmia suspend alarms were examined in a pre-and post-QI study assessing whether daily skin electrode changes reduced these types of alarms. The investigators showed that this type of alarm decreased by 60%

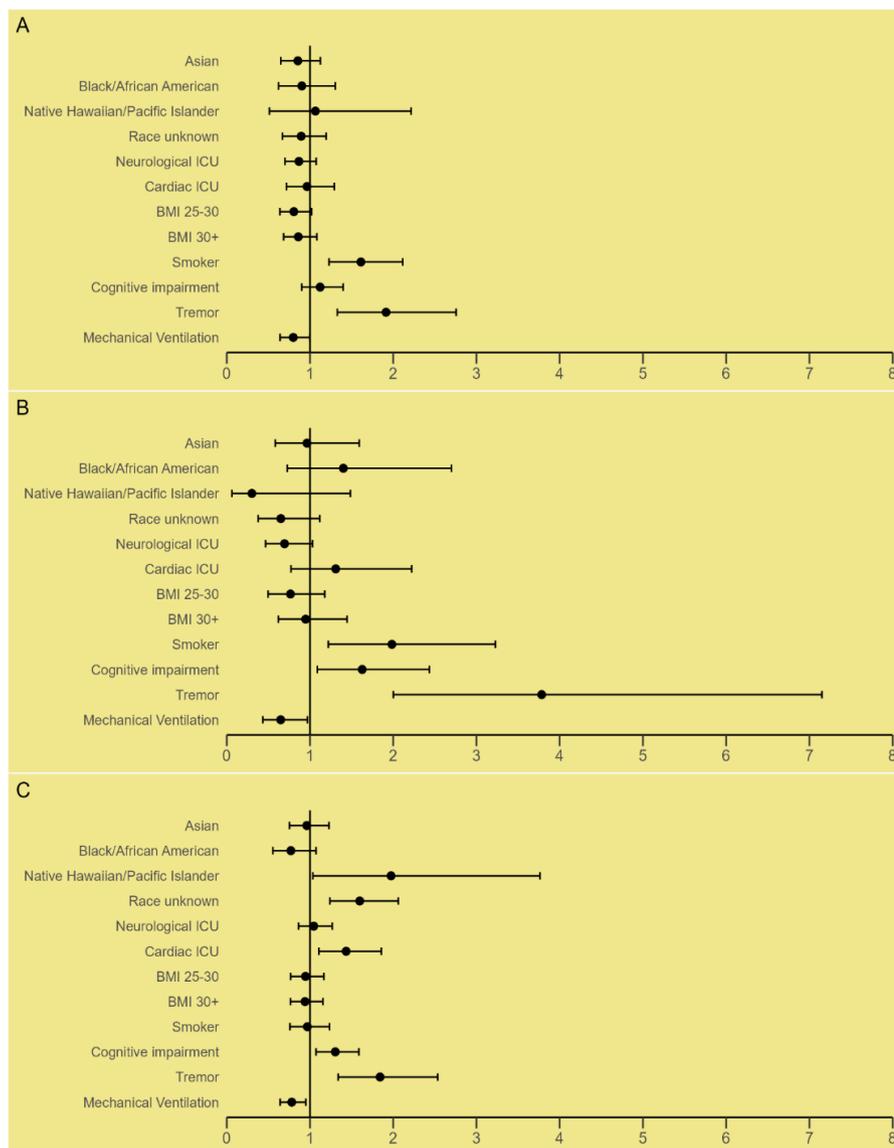


Figure 2. Forest plots of each technical alarm type: (a) artefact, (b) arrhythmia suspend, & (c) ECG leads fail.

in the medical progressive care unit and 74% in the cardiology care unit following the intervention. This suggests that daily skin electrode changes may reduce this type of alarm. However, patient and/or clinical characteristics associated with this type of alarm were not reported.

In a study by Graham et al. (2010), arrhythmia suspend alarms were examined pre- and post-QI implementation focused on several initiatives (i.e., changing default settings, education on individualising patient default settings, adjusting audible alarms, and a software modification) in

the progressive care unit. Prior to the intervention, there were 634 arrhythmia suspend alarms, and after the intervention, they increased to 1,116. It is unclear why there were more of these types of alarms post-QI implementation, but overall alarm rates for a multitude of other alarm types were reduced post-QI implementation. One intervention used by the investigators was to adjust alarm settings (e.g., warning [foghorn tone] to an inaudible message) to reduce nuisance alarms (true but not actionable). However, it was not described whether arrhythmia suspend was adjusted in their study from a warning

alarm to an inaudible message alert. If this adjustment was made, this might explain why there were more arrhythmia suspend alarms post-intervention. For example, if an alarm tone was not generated, the nurse would be less likely to solve this issue because it was set as an inaudible message alert. This type of technical alarm is generated when certain conditions are present, such as ECG leads off or, in the case of the monitor in place during this study, sustaining artefact >20 seconds in the prior 30 seconds. This indicates that arrhythmia analysis has been suspended (off), which has important clinical implications as an arrhythmia might be missed.

In our study, only 0.6% of the patients had this type of alarm, and the mean and median time a patient was in this alarm condition was 10 minutes and 2 minutes, respectively. We found that patients who were current smokers at admission and those with cognitive impairment or tremors were more likely to have this type of technical alarm. Therefore, nurses should assess for these patient characteristics and, if indicated, consult with the care team on strategies to minimise the effects of these clinical features (i.e., nicotine withdrawal treatment) if possible. These types of patients may also benefit from daily skin electrode changes, which have been shown to reduce artefacts that can create this type of alarm (Cvach et al. 2013; Sendelbach et al. 2015).

ECG Leads Fail

Contrary to artefact and arrhythmia suspend, all seven prior published studies that were relevant to compare to our study had measured ECG leads fail alarms (Albert et al. 2015; Cvach et al. 2013; Drew et al. 2014; Graham and Cvach 2010; Harris et al. 2017; Shue and Ortiz 2019; Watanakeeree et al. 2021). In the studies by Shue and Ortiz (2019) and Sendelbach et al. (2015), ECG leads fail alarms were measured, but grouped together with other types of technical alarms (e.g., no signal or telemetry battery low) or measured per day as a mean number of all ECG alarms. These two studies implemented several tests of change but it's not clear how these

interventions specifically affected ECG leads fail alarm rates. Our study was designed to measure the occurrence rate of ECG leads fail alarms, which was found to be 2.2% (12,367) of all of the technical alarms. This type of data could be helpful in determining whether a reduction in ECG lead fail/off alarms are due to various interventions proposed in previous studies.

Two QI implementation projects had a specific focus on ECG leads fail/off alarms through several interventions, including daily electrode changing, custom alarm parameters, software modification, and clinician education (Cvach et al. 2013; Graham and Cvach 2010). Both studies by Cvach et al. (2013) and Graham et al. (2010) demonstrated an increase in the total number of ECG lead fail alarms by 39 and 314, respectively. In these instances, nurse susceptibility to alarm fatigue and exposure to audible alarms may have been reduced, but arrhythmia detection may also have been impacted. It's unclear whether this was a significant issue since the time in this alarm condition nor clinical features associated with this alarm condition were reported. Within our dataset, we found that documented cognitive impairment and tremors were associated with ECG lead failure. The mean time within this alarm condition was almost 20 minutes. However, the vast majority of lead fail alarms were between 2 seconds and 5 minutes. These findings offer important evidence that these types of alarms are generated after only a short duration of time in this alarm condition. One solution may be to add a delay for these types of alarms in the configuration setting. However, the optimal delay time needs further investigation to ensure patient safety.

In the study by Drew et al. (2014), 90,547 single lead fail alarms (inaudible messages) occurred over a one-month timeframe. It's important to note that ECG leads fail, which we report, will sound an audible foghorn tone. While their study only provided data for single ECG lead failure, our study showed that 99.4% of ECG lead failure alarms were between 2 seconds and 5 minutes in duration. Some of these are likely to be considered a nuisance and

exacerbate the level of noise and possibly alarm fatigue within a busy ICU. In a secondary data analysis of this study in patients with an LVAD, there were 854 ECG lead fail alarms during a one-month time period (Watanakeeree et al. 2021). Even though this study provided valuable insight into a clinical feature that affected technical alarm rates in LVAD patients, generalisability is reduced since only three patients were examined.

ECG leads fail alarms can pose an increased risk for alarm fatigue and may compromise patient safety. A randomised study examining the difference in alarm events between disposable and reusable lead wires showed a decrease in the total number of all false alarms (i.e. no telemetry, leads off/fail artefact, and false crisis) when using disposable lead wires (Albert et al. 2015). Non-inferiority statistical analysis also demonstrated that disposable lead wires might be a reasonable approach as a potential solution for reducing technical alarms during continuous ECG monitoring.

Alarm Duration

For each type of technical alarm, the vast majority were found to be between two seconds and 5 minutes (99.2-99.4%). Duration of alarms between 5 minutes and 15 minutes was extremely uncommon (0.1-0.6%), which may suggest that current technical alarm algorithms are too sensitive and should be designed with a delay. As previously discussed, our evidence shows that clinical features (e.g., current smoker, documented tremor, or cognitive impairment, etc.) are associated with higher incidence rates for certain types of technical alarms. Technical alarm thresholds should also be adjusted with the goal of reducing nuisance alarms caused by known clinical features from the patient's EHR.

Limitations

Several limitations warrant consideration. While we provide new information on the number and types of technical alarms, we did not correlate technical alarms with a patient's status at the time of the alarm (i.e., bathing, changing electrodes,

repositioning, tests at the bedside, etc.). This means the nurse may have been at the bedside with the patient, and the alarm had minimal impact on alarm burden/fatigue. Because only one vendor's monitor was used, we do not know if our findings are generalisable to other device manufacturers. The study's retrospective design did not allow us to evaluate how alterations in alarm settings (e.g., turn off, adjust to inaudible setting) would impact the number of alarms identified. Despite these limitations, our study represents the most comprehensive evaluation of technical alarms in a consecutive sample of ICU patients done to date.

Conclusion

The vast majority of technical alarms were for artefact. Arrhythmia suspend (software off) due to sustained artefact was uncommon. However, the mean time patients were in this technical alarm condition was 10 minutes, which could be important for ICU patients since arrhythmia detection may be compromised. Individual alarms lasted only seconds, which suggests that technical alarms are too sensitive and should be re-designed with a delay (e.g., 5 minutes) before alarming. Patients who were current smokers at admission were more likely to have artefact and arrhythmia suspend alarms. Having a tremor was associated with all three types of technical alarms. Documented cognitive impairment was associated with arrhythmia suspend and ECG leads fail alarms. Patients treated with mechanical ventilation had fewer alarms (all three types). Patients with these features may require more guided alarm management strategies and/or treatment for nicotine withdrawal, or tremor as they are more likely to generate technical alarms.

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Conflict of Interest

None.

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